Right Ventricular Failure in Idiopathic Pulmonary Arterial Hypertension

Is Associated with Inefficient Myocardial Oxygen Utilization

Wong et al: Inefficient O₂ Use by Failing Right Heart in PAH

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[32] Nuclear cardiology and PET
Abstract

**Background**—In idiopathic pulmonary arterial hypertension (IPAH), increased right ventricular (RV) power is required to maintain cardiac output. For this, RV O\textsubscript{2} consumption (MVO\textsubscript{2}) must increase by augmentation of O\textsubscript{2} supply and/or improvement of mechanical efficiency - ratio of power output to MVO\textsubscript{2}. In IPAH with overt RV failure, however, there is evidence that O\textsubscript{2} supply (perfusion) reserve is reduced, leaving only increase in either O\textsubscript{2} extraction or mechanical efficiency as compensatory mechanisms. We related RV mechanical efficiency to clinical and hemodynamic parameters of RV function in IPAH patients and associated it with glucose metabolism.

**Methods and Results**—The patients included were NYHA II (n=8) and III (n=8). They underwent right heart catheterisation, MRI and H\textsuperscript{2}\textsuperscript{15}O, \textsuperscript{15}O\textsubscript{2}, C\textsuperscript{15}O\textsuperscript{2} and \textsuperscript{18}FDG-PET. RV power and O\textsubscript{2} supply were similar in both groups (NYHA II vs III: 0.54±0.14 vs 0.47±0.12 J/s; and 0.109±0.022 vs 0.128±0.026 ml O\textsubscript{2}/min/g, respectively). RV O\textsubscript{2} extraction was near-significantly lower in NYHA II compared with NYHA III (63±17% vs 75±16%, respectively, P=0.10). As a result, MVO\textsubscript{2} was significantly lower (0.066±0.012 vs 0.092±0.010 ml O\textsubscript{2}/min/g, respectively, P=0.006). RV efficiency was reduced in NYHA III (13.9±3.8%) compared to NYHA II (27.8±7.6%, P=0.001). Septal bowing, measured by MRI, correlated with RV efficiency (r=-0.59, P=0.020). No relation was found between RV efficiency and glucose uptake rate. RV mechanical efficiency and ejection fraction were closely related (r=0.81, P<0.001).

**Conclusions**—RV failure in IPAH was associated with reduced mechanical efficiency that was partially explained by RV mechanical dysfunction, but not by a metabolic shift.

**Key Words:** idiopathic pulmonary arterial hypertension, right ventricular mechanical efficiency, oxygen supply and consumption, right ventricular failure, positron emission tomography
In idiopathic pulmonary arterial hypertension (IPAH), both pulmonary vascular resistance and right ventricular (RV) afterload increase progressively. This causes RV hypertrophy and may lead to RV failure. To maintain cardiac output during the increasing afterload in IPAH, sufficient power output has to be generated by the RV, which requires more O2. Recently, however, Gomez et al.1 observed stress-induced ischemia in the RV wall of a subset of PAH patients with overt RV failure and suggested an association between RV ischemia and dysfunction. The same study also suggests that RV perfusion reserve at rest may be exhausted in severe PAH, which would restrict the RV in a further adaptive response. If perfusion reserve is indeed limited, the only possibility for the RV to meet its energy requirements is to increase its mechanical efficiency, which is proportional to the ratio of ventricular power output and myocardial O2 consumption (MVO2). However, unlike left ventricular (LV) disease and heart failure where mechanical efficiency is reduced,2-10 mechanical efficiency in overt RV failure is unknown.

Due to the vascular anatomy of the human RV, its venous PO2 has not been determined invasively. Recently, we demonstrated that O2 extraction fraction (OEF) of the thickened RV wall in IPAH, can be non-invasively measured using the spatial resolution of state-of-the-art positron emission tomography (PET) scanners and 15O2 and C15O tracers.11 Here, we also measured RV perfusion, using H215O-PET next to OEF to calculate RV MVO2.12

The purposes of this study were to (1) determine the relationship between RV power output and MVO2 in IPAH patients and (2) relate RV mechanical efficiency to RV function using both clinical and functional assessments in IPAH patients. We also determined whether mechanical RV dysfunction and RV glucose uptake rate related to the RV efficiency that was found.
Methods

Patients

26 IPAH were eligible for study. Five patients refused to participate and 5 other patients gave consent but were subsequently withdrawn due to emergence of severe clinical condition (n=2; hemoptysis and endocarditis) or because of unsuccessful canulla placement in the radial or brachial artery (n=3). In total, 16 patients were included, of which fifteen patients were on optimal treatment and diagnosed with IPAH for a median time of 3 years, ranging from 2 months to 7 years. One patient was newly diagnosed with severe IPAH and included right before start of drug treatment. All patients continued receiving treatment (Table 1). Exclusion criteria were: known history of coronary artery disease or diabetes mellitus, atrial fibrillation, anaemia (hemoglobin <0.13 g/mL). Assessment of the WHO 1998’s adapted NYHA classification, was performed prior to study participation by the clinicians responsible for the patient (AVN and AB). The protocol was approved by the Medical Ethics Review Committee of VU University Medical Center. Each patient gave written informed consent prior to study. YYW and GR analysed the images blinded for patient’s clinical state.

Study design

All patients underwent right heart catheterization (RHC), cardiac magnetic resonance imaging (cMRI) and PET that consisted of three consecutive scans using H$_2^{15}$O, $^{15}$O$_2$ and C$^{15}$O to measure myocardial perfusion or blood flow (MBF), OEF and MVO$_2$ and fractional blood volume, respectively (Figure 1). $^{15}$O-PET scans were performed 2 hours after a light breakfast. One day after the $^{15}$O-PET scans, a $^{18}$F-2-fluoro-2-deoxy-D-glucose ($^{18}$FDG) scan was performed to quantify myocardial glucose uptake rate (Mrglu) (Figure Suppl-1A-B and Supplement text). When possible, RHC, cMRI and PET studies were performed within one week of each other. In three subjects, for logistical or personal reasons, the interval between
RHC and PET was 20 to 55 days, and between cMRI and PET 20 to 36 days. As these patients had stable IPAH under drug treatment, i.e. less than 10% change in 6MWD over 6 months prior to inclusion (5±3%), no change in medical therapy or NYHA class, the interval was considered acceptable.

**PET imaging protocol**

Patients received a cannula in the radial or brachial artery for blood sampling.

*Data acquisition* The protocol for cardiac H$_2^{15}$O and C$^{15}$O scans has been described previously.$^{12}$ Briefly, scans were performed in 2D acquisition mode using an ECAT EXACT HR+ scanner (Siemens/CTI, Knoxville, TN, USA). After transmission scan, used to correct all subsequent scans for tissue attenuation, subjects underwent three consecutive scans as shown in Figure 1. First, a dynamic emission scan (10 min, 40 frames with progressive increase in duration) was started simultaneously with injection of 1100 MBq H$_2^{15}$O. A second identical emission scan was started at the same time as a bolus inhalation 7 GBq $^{15}$O$_2$. During the $^{15}$O$_2$ scan, five arterial blood samples were obtained to measure recirculating H$_2^{15}$O concentration.$^{11}$ An additional arterial sample was drawn to determine arterial O$_2$ content. Finally, a 6 min static emission scan was acquired, starting 1 min after end of bolus inhalation of 4 GBq C$^{15}$O gas to allow imaging of ventricular blood volumes. Approximately 20% of the administered radioactivity during $^{15}$O$_2$ and C$^{15}$O inhalation is taken up by the blood.$^{13}$ During all scans systemic blood pressure and peripheral saturation were registered at set intervals. Heart rate and ECG were monitored continuously.

*Image processing and data analysis* All emission data were reconstructed as previously described.$^{12}$ The anatomical tissue fraction (ATF) images, generated by subtracting the C$^{15}$O blood pool image from transmission image,$^{14}$ were resliced into short-axis images according to anatomic axes of the LV. The same reslicing parameters were applied to both
dynamic H$_2^{15}$O and $^{15}$O$_2$ images. Using ATF images, RV wall regions of interest (ROIs) were defined on basal, distal and apical planes (Figure 2). These ROIs were projected onto dynamic H$_2^{15}$O and $^{15}$O$_2$ images to generate time-activity curves. Next, volume weighted averages of basal, distal and apical time-activity curves were averaged. MBF was determined from these average time-activity curves using the standard single tissue compartment model.$^{15}$ OEF was determined from $^{15}$O$_2$ scan using dynamic implementation$^{11}$ of a previously described model,$^{14}$ re-using MBF, perfusable tissue fraction, arterial blood volume and RV spill-over as determined from the H$_2^{15}$O scan and applying a correction for spill-over from activity in the pulmonary gas volume as described previously.$^{16}$ $^{15}$O$_2$ input function was based on volume of interest drawn in ascending aorta and corrected for contribution of recirculating water measured in the arterial blood samples.

**Hemodynamic and oxidative calculations**

A brief description is provided for both RHC and cMRI in the Supplement.

RV ejection fraction (EF) was derived as the ratio of stroke volume (SV, assessed from aortic flow) to RV end-diastolic volume. RV post-systolic isovolumic period, which is the time between pulmonary valve closure and tricuspid valve opening, was determined in the two-chamber view described previously and corrected for RR-time.$^{17}$ The interventricular septum plays an important role in RV power generation in PAH. Therefore, total septal mass, determined by LV mass minus LV free wall mass, was divided into a right and left septal mass assuming that the right and left part of the septal masses are proportional to their free wall counterparts. The right septal part was included to the RV wall mass in the following calculations.
Right ventricular power Combining hemodynamic data from both RHC and cMRI, the power (J/s) of the RV was calculated as:

\[
Power = HR \cdot mPAP \cdot SV \cdot 2.22 \cdot 10^{-6}
\]  \hspace{1cm} (Eq 1)

where HR is heart rate in beats per minute and mPAP in mmHg; SV, in mL, was assessed from the difference between LV end-diastolic volume and end-systolic volume, which was found to be equally accurate as the forward aortic flow for SV assessment in IPAH.\(^{18}\) The factor \(2.22 \cdot 10^{-6}\) converts mmHg·L/min to J/s. Only mean power output is used in the present study. Saouti et al. showed total power equals 1.23 times mean power\(^{19}\) and, thus, does not affect the results qualitatively.

Right ventricular oxygen consumption and supply Regional myocardial \(\text{O}_2\) consumption (MVO\(_2\) in ml/min/g cardiac tissue) was calculated for RV as follows:\(^{14}\)

\[
MVO_2 = OEF \cdot MBF \cdot CaO_2
\]  \hspace{1cm} (Eq 2)

where \(CaO_2\) is arterial \(\text{O}_2\) content (mL \(\text{O}_2\)/mL blood).\(^{14}\) Myocardial \(\text{O}_2\) supply (ml/min/g) was calculated as \(MBF \times CaO_2\).

Mechanical efficiency was calculated from the ratio of RV power output (eq 1) and MVO\(_2\) (eq 2). As MVO\(_2\) in eq 2 is calculated per gram, RV mass is included here for calculation of MVO\(_2\) by whole RV. To convert RV MVO\(_2\) to units of metabolic power (J/s), it was multiplied by the caloric equivalent of \(\text{O}_2\): 1 mL of \(\text{O}_2\)/min corresponds to about 0.34 J/s, assuming that RV oxidizes free fatty acid and glucose equally:

\[
\text{Mechanical efficiency} = \frac{Power}{MVO_2 \cdot RVmass \cdot 0.34} \times 100\% \hspace{1cm} (Eq 3)
\]
Statistical analysis

All results are expressed as mean±SD. The two groups (i.e. NYHA II and III) were compared using t-tests; the non-parametric Mann-Whitney U test was used where indicated. Pearson’s correlation was performed where necessary. All statistics were performed using Prism 5 for Windows (GraphPad Software, San Diego CA). P<0.05 was considered significant.
Results

Patient characteristics and hemodynamics are summarized in Table 1; some parameters are also shown in Figure 3. In accordance with severity of IPAH, NYHA III patients had lower SV and CO (Figure 3A), despite higher heart rate as compared to NYHA II. Mean PAP was near-significantly higher in NYHA III as compared to II (Figure 3B; P=0.083, Mann-Whitney-U). PVR was increased in NYHA III, whereas RV mass was similar in the two groups. RVEF and SvO₂ were lower in NYHA III. Six-minute walk distance was not significantly lower in the severely ill.

PET derived parameters for the RV per cardiac mass are shown in Table 2. Both MBF (corrected for RV mass, Figure 3C) and OEF (Figure 3D) were not significantly higher in the NYHA III (MBF: P=0.088, t-test; OEF: P=0.105, Mann-Whitney U). There was, however, a significantly higher MVO₂ per gram (Table 2). In contrast, RV O₂ supply per gram RV was similar in NYHA II and III patients (Table 2). For total RV, MVO₂ was also higher in the severely ill (Figure 3F), whereas RV power was not significantly lower (Figure 3E). This led to a significant reduction of RV efficiency by ~50% in the NYHA III patients compared with the NYHA II patient group (Figure 3G).

A tight relationship was found between the mechanical efficiency and RVEF, a hemodynamic index of systolic RV function parameter (Figure 4, r -0.81, P<0.001). There was also a high correlation between RV efficiency and SvO₂ (r 0.76, P<0.001).

In search for an underlying mechanical cause for the reduced efficiency, post-systolic isovolumic period was plotted against the RV efficiency, showing a negative correlation (r -0.594, P=0.020, Figure 5). No correlation was found between the RV MRglu and RV efficiency (r -0.38; P=0.18, Figure Suppl-1C).
Discussion

In the present study, we demonstrate that RV mechanical efficiency is lower in NYHA III than in NYHA II patients (Figure 3G), indicating a decrease with progression of IPAH. In addition, the strong relation between RVEF and mechanical efficiency (Figure 4) stresses the fact that decreasing mechanical efficiency is a characteristic for deterioration of RV function in IPAH. The reduced efficiency in NYHA III patients is not related to RV power output as this was similar between the two groups (Figure 3E), but NYHA III patients had higher MVO2 of both total RV (Figure 3F) and per unit RV mass (Table 2) as compared to NYHA II.

To the best of our knowledge, there are no previous data on human OEF and perfusion of the normal RV to compare with our patient data. Based on canine studies, normal RV OEF has been estimated as 45 to 50%, indicating that the RV has a substantially higher O2 extraction reserve than the left heart (OEF values are 60 to 80% in healthy men). Additionally, Hart et al. demonstrated that during heavy exercise, RV O2 utilization increases initially by maximizing OEF before coronary reserve is mobilized. Interestingly, we found a mean RV OEF of 69 ± 17% in our IPAH patients (Figure 3D) approximating that of normal LV. Our data suggests that, in analogy with the normal (canine) RV during strenuous exercise, the pressure overloaded RV in IPAH has already a reduced O2 extraction reserve at rest and resting O2 demand becomes predominantly dependent on perfusion. We found similar MBF in the hypertrophied RV between mild and severe IPAH. We, therefore, hypothesize that the dysfunctional RV is unable to increase its perfusion in severe PAH; and thus O2 supply cannot increase to meet a higher O2 demand (e.g. during physical exercise). RV ischemia is then the result, which is in accordance with the observation by Gomez et al. who demonstrated stress-induced RV wall ischemia in IPAH patients with severe heart failure. The high RV OEF that we found may also increase the risk to develop hypoxia in the hypertrophied RV cardiomyocytes.
RV power in the NYHA III group was similar to NYHA II (Figure 3E), despite lower SV and CO (Table 1, Figure 3A), but we have to take into account that RV power is significantly higher compared to the normal RV (Figure Suppl-2). Previous studies also demonstrated that patients with advanced IPAH had significantly reduced CO, but similar mPAP as compared to mild IPAH. The RV power that can be calculated from the data provided in these studies is also not significantly lower in the progressively IPAH patients, which is in agreement to our data. It follows from the lower CO and unchanged mPAP that PVR is higher in the NYHA III patients (Table 2). Apparently, RV power output cannot be increased in advanced IPAH to maintain CO and SV, which is a sign of RV failure. This is further supported by the tight relationship between RVEF and mechanical efficiency (Figure 4), which has also been shown in patients with ischemic LV heart disease. Reduced SvO₂ is a strong prognostic determinant in IPAH, as it is associated with a decreased cardiac output in the severely ill. It is noticeable that RV efficiency independently correlates well with SvO₂, emphasizing once more that mechanical efficiency is a strong indicator for RV function.

Potential underlying mechanisms of mechanical inefficiency at the mechanical and/or cardiomyocyte level Mechanical dysfunction can be due to tricuspid regurgitation, septal bowing, asynchronous activation and/or diastolic dysfunction. Power output loss due to tricuspid regurgitation, however, was small and did not influence the mechanical efficiency in our present study (Supplement Table 1). In contrast, we did find a weak, but significant, inverse relation between prolonged post-systolic isovolumic period and reduced RV efficiency (Figure 5). Based on recent insight, this prolonged period is related to the post-systolic RV isovolumetric contraction period, rather than a prolonged diastolic relaxation time, indicating the presence of abnormal increased RV wall tension in these patients. This prolonged period is visible on echocardiography or cardiac MRI as leftward septal bowing
after pulmonary valve closure, increasing RV MVO$_2$ without ejection of blood. The low correlation coefficient found between this period and RV efficiency, however, suggests that the reduced efficiency cannot be explained by this prolonged isovolumic contraction period alone. Prostacyclin was shown to improve the right arterioventricular coupling through reduction of arterial elastance.$^{27}$ This treatment was more common in the NYHA III group (Table 1). Nevertheless, it did not prevent the reduced RV efficiency in our patient population. Furthermore, it is possible that myocardial fibrosis contributes to a reduced mechanical efficiency. Blyth et al. found that patients with a lower RVEF had more myocardial fibrosis than patients with a preserved RVEF.$^{28}$

Additional causes for reduced efficiency must be sought at the cardiomyocyte level in advanced RV failure. Unfortunately, it is not possible to obtain RV cardiac tissue in our study population for histological analysis of morphological changes or capillary density. Preclinical PH studies, however, show that RV cardiomyocytes are enlarged with reduced capillary density.$^{29,30}$ The oxygen diffusion distance is increased due to these changes, which may be an underlying cause for reduction in efficiency. Indeed, we recently showed a similar reduction in mechanical efficiency in the isolated, hypertrophied RV papillary muscle obtained from an experimental PH model.$^{31}$

Chronic heart failure takes place with a metabolic shift from free fatty acids to glucose oxidation.$^{3,4,8}$ This shift was demonstrated also in the hypertrophied right ventricle in experimental and clinical PAH studies.$^{32-34}$ In theory, the efficiency should increase because glucose oxidation yields more energy than fat oxidation per mole of oxygen. However, in heart failure the shift to glucose oxidation seems to concur with the presence of reduced mechanical efficiency, suggesting that the glucose shift is a secondary phenomenon to the diminished efficiency. We also measured the glucose metabolism in our patients and found that the RV glucose uptake rate was similar in NYHA II and NYHA III patients (P=0.18,
Figure Suppl-1C). The increased MVO₂ to power output in severe IPAH suggests inefficient O₂ utilization by the failing RV due to cellular processes in which O₂ is used for processes other than ATP production for contraction, e.g. ion pumps, protein turnover, mitochondrial uncoupling or oxygen radical formation. Indeed, local administration of XO inhibitor, NO-synthase inhibitor or vitamine C (a reactive oxygen species scavenger) have been shown to ameliorate the low LV efficiency in cardiomyopathy patients, as well it was reported to attenuate RV failure in a PH rat model. Future studies on the isolated RV papillary muscle of PH rats are warranted to test whether these substances also improve the reduced RV efficiency found in PH.

Our data indicate that clinical judgement, i.e. NYHA class – a well known prognostic determinant for survival in PAH – is a reflection of the RV mechanical inefficiency. We hypothesize that there is not only a mere association between NYHA class and mechanical efficiency, but that RV inefficiency is an underlying factor causing clinical deterioration and that it plays a central role in RV failure in IPAH.

Limitations We acknowledge that the present study lacks a control group. Unfortunately, the normal RV wall is too thin for accurate measurements of MBF and OEF, given the spatial resolution of current PET scanners. Nevertheless, we were able to include patients with sufficiently different disease severity to discover the significant correlation between RV efficiency and RVEF. Ideally, all measurements required for calculation of mechanical efficiency should be acquired simultaneously. This was not possible because of the variety of measurement modalities used. However, only clinically stable IPAH patients participated in this study and most measurements were performed within one week. We have chosen to include part of the septum in the RV myocardial mass. To date, it is not clear how much it contributes to RV pumping and O₂ consumption in IPAH. We performed calculations of RV efficiency also by taking either the full septum into account or only the RV free wall
and found qualitatively similar results (Figure Suppl-3). Finally, it would be interesting to compare the RV mechanical efficiency between different PAH subgroups. Differences in RV mechanical efficiency may be an underlying factor to explain the differences found in the hemodynamics and prognosis between IPAH patients and patients with PAH secondary to scleroderma or Eisenmenger syndrome.

**Conclusion** RV mechanical efficiency is reduced in severe IPAH compared with milder stages of the disease process and is only partially explained by RV mechanical dysfunction, but not by a metabolic shift to glucose oxidation. The reduction in mechanical efficiency is strongly correlated with RVEF, implying that the increased O₂ use relative to power output is a feature of RV failure.
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Disclosures

A.V.N reports to have received speaker’s and advisory board grants from Actelion and Pfizer, and received speaker’s grant from GlaxoSmithKline. A.B. reports to have received a speakers’s grant from Pfizer. The other authors declare that they have conflicts of interest.
References


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Table 1. Patient characteristics and hemodynamics

<table>
<thead>
<tr>
<th>NYHA</th>
<th>all</th>
<th>II (n = 8)</th>
<th>III (n = 8)</th>
<th>P</th>
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<tr>
<td>Age (yrs)</td>
<td>44.8 ± 12.8</td>
<td>42.4 ± 12.4</td>
<td>47.1 ± 13.6</td>
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</tr>
<tr>
<td>Female / Male</td>
<td>15 / 1</td>
<td>7 / 1</td>
<td>8 / 0</td>
<td>-</td>
</tr>
<tr>
<td>Prostacyclin all / single treatment (n)</td>
<td>2 / 0</td>
<td>4 / 2</td>
<td></td>
<td></td>
</tr>
<tr>
<td>ERA all / single treatment (n)</td>
<td>7 / 3</td>
<td>3 / 0</td>
<td></td>
<td></td>
</tr>
<tr>
<td>PDE5 all / single treatment (n)</td>
<td>4 / 1</td>
<td>4 / 1</td>
<td></td>
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<tr>
<td>6MWD (m)</td>
<td>455 ± 116</td>
<td>496 ± 104</td>
<td>415 ± 119</td>
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<td>mRAP (mmHg)</td>
<td>9 ± 7</td>
<td>5 ± 5</td>
<td>13 ± 8</td>
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<tr>
<td>mPAP (mmHg)</td>
<td>52 ± 14</td>
<td>46 ± 12</td>
<td>57 ± 14</td>
<td>ns</td>
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<td>Heart rate (bpm)</td>
<td>76 ± 15</td>
<td>67 ± 63</td>
<td>85 ± 15</td>
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<tr>
<td>Stroke volume (mL)</td>
<td>64 ± 24</td>
<td>81 ± 16</td>
<td>48 ± 19</td>
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<td>Cardiac output (L/min)</td>
<td>4.6 ± 1.2</td>
<td>5.3 ± 0.8</td>
<td>3.9 ± 1.1</td>
<td>0.009</td>
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<tr>
<td>RV mass (g)</td>
<td>102 ± 29</td>
<td>93 ± 35</td>
<td>111 ± 19</td>
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</tr>
<tr>
<td>RV EDV (mL)</td>
<td>165 ± 50</td>
<td>154 ± 55</td>
<td>177 ± 46</td>
<td>ns</td>
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<tr>
<td>RV EF (%)</td>
<td>35 ± 16</td>
<td>46 ± 15</td>
<td>25 ± 9</td>
<td>0.002</td>
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<tr>
<td>PVR (dyn·s·cm⁻⁵)</td>
<td>697 ± 345</td>
<td>504 ± 222</td>
<td>890 ± 279</td>
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<td>NTproBNP (ng/L)</td>
<td>1242 ± 1777</td>
<td>540 ± 669</td>
<td>1693 ± 2330</td>
<td>ns</td>
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<tr>
<td>SvO₂ (%)</td>
<td>67 ± 6</td>
<td>71 ± 3</td>
<td>63 ± 4</td>
<td>0.002</td>
</tr>
<tr>
<td>Arterial O₂ content</td>
<td>0.18 ± 0.02</td>
<td>0.18 ± 0.02</td>
<td>0.18 ± 0.01</td>
<td>ns</td>
</tr>
</tbody>
</table>

Mean ± SD; ERA endothelin receptor antagonist, EDV end diastolic volume, EF ejection fraction, mPAP mean pulmonary artery pressure, mRAP mean right atrial pressure, PDE5 phosphodiesterase type 5 inhibitors, PVR pulmonary vascular resistance, 6MWD six-minute walk distance, RV right ventricle, SvO₂ mixed venous O₂ saturation. P values were tested using t-test.
**Table 2.** Perfusion and O$_2$ consumption of RV per unit mass measured by PET

<table>
<thead>
<tr>
<th>NYHA</th>
<th>II ($n = 8$)</th>
<th>III ($n = 8$)</th>
<th>$P$</th>
</tr>
</thead>
<tbody>
<tr>
<td>MBF (mL/min/g)</td>
<td>$0.61 \pm 0.15$</td>
<td>$0.71 \pm 0.16$</td>
<td>ns</td>
</tr>
<tr>
<td>O$_2$ supply (mL/min/g)</td>
<td>$0.109 \pm 0.022$</td>
<td>$0.128 \pm 0.026$</td>
<td>ns</td>
</tr>
<tr>
<td>MVO$_2$ (mL/min/g)</td>
<td>$0.066 \pm 0.012$</td>
<td>$0.092 \pm 0.010$</td>
<td>$&lt; 0.001$</td>
</tr>
</tbody>
</table>

Mean $\pm$ SD; MBF myocardial blood flow, MVO$_2$ myocardial oxygen consumption. $P$ values were tested using t-test.
Figure Legends

Figure 1. PET protocol time scheme.
C\textsuperscript{15}O scan was initiated 1 minute after end of C\textsuperscript{15}O inhalation. See text for explanation.

Figure 2. Example of a cMRI and C\textsuperscript{15}O-PET image of an IPAH patient with NYHA III.
Cardiac MRI image of a patient’s heart with severe IPAH at short axis view, cut at mid level of the heart (panel A). C\textsuperscript{15}O-PET image, reconstructed as an attenuation tissue fraction, a so-called ‘negative image’ of the ventricular blood volumes after inhalation of C\textsuperscript{15}O (panel B). Using this image the RV wall was defined, depicted as a marked region in panel C. The RV wall regions of base, mid and apical levels were combined to a RV wall volume. This was then projected onto the dynamic H\textsubscript{2}\textsuperscript{15}O and \textsuperscript{15}O\textsubscript{2} images for quantification RV blood flow and O\textsubscript{2} extraction, respectively.

Figure 3. Overview of the determinants of RV mechanical efficiency.
Primary measurements are cardiac output (panel A) measured by cardiac MRI, mean pulmonary artery pressure (mean PAP, panel B) acquired by right heart catheterization, myocardial blood flow (panel C) that was measured by H\textsubscript{2}\textsuperscript{15}O-PET and RV O\textsubscript{2} extraction fraction (panel D) obtained by \textsuperscript{15}O\textsubscript{2}-PET. RV power (panel E) is derived from cardiac output and mean PAP (Equation 1 Methods Section) and myocardial O\textsubscript{2} consumption (panel F) from O\textsubscript{2} extraction fraction and myocardial blood flow (equation 2). Mechanical efficiency (panel G) is the ratio of power and myocardial O\textsubscript{2} consumption (equation 3). There was a trend toward significant difference for mean pulmonary artery pressure (P=0.083, Mann-Whitney U), O\textsubscript{2} extraction fraction (P=0.105, Mann-Whitney U) and myocardial blood flow (P=0.088). Each panel shows results for NYHA II (left bar) and III (right bar) patients. **P<0.01; ***P<0.001.
Figure 4. RV efficiency as function of RV ejection fraction.

A strong correlation exists between the two parameters (see text). Filled circles are NYAH II; open circles are NYHA III patients. Regression line (thick broken line) and 95% confidence band (thin dashed lines) are shown.

Figure 5. Plot of the post-systolic isovolumic period (PS-IVP), corrected for RR-time (in fraction of heart cycle) against the RV mechanical efficiency.

The dashed line represents the best fit to the data. $R^2$ was 0.35. In one patient, this period was not obtained. Filled circles are NYAH II; open circles are NYHA III patients. Regression line (thick broken line) and 95% confidence band (thin dashed lines) are shown.
Right Ventricular Failure in Idiopathic Pulmonary Arterial Hypertension Is Associated with Inefficient Myocardial Oxygen Utilization

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Anco Boonstra, MD, PhD2; Adriaan A. Lammertsma, PhD1; Nico Westerhof, PhD12;
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Supplement Methods and Results

Right heart catheterization
The protocol has been detailed previously. Briefly, under continuous ECG monitoring, a balloon-tipped, flow-directed 7.5F Swan-Ganz VIP+ catheter (834HF75, Edwards Lifesciences Corporation, Irvine, CA, USA) was inserted in patient’s internal jugular vein. Cardiac output (CO) was measured by means of thermodilution. Blood was sampled from the main pulmonary artery to measure mixed venous oxygen saturation (SvO₂). Pulmonary vascular resistance (PVR) was calculated as: (mPAP-PCWP)/CO, where mPAP is mean pulmonary arterial pressure and PCWP pulmonary capillary wedge pressure.

Cardiac magnetic resonance imaging
Scanning protocol is described previously. Cardiac MRI scans were acquired on a Siemens 1.5 T Sonata scanner or Siemens 1.5 T Avanto whole body scanner (Siemens Medical Solutions, Erlangen, Germany). RV volumes and mass were measured from the stack of short axis images by manual detection of the endocardial and epicardial borders of RV on each slice using MR-Analytical Software System (Media, Leiden, Netherlands). RV end-diastolic, end-systolic volumes and RV free wall mass were calculated.
**Effect tricuspid regurgitation on loss of right ventricular power output**

Six idiopathic pulmonary arterial hypertension (IPAH) patients (NYHA II, n=1; NYHA III, n=5) had moderate to severe tricuspid regurgitation found on echocardiography. ‘Backward’ volume is the amount of regurgitated volume from the right ventricle into the right atrium, calculated by the difference between the right ventricular (RV) end diastolic volume and RV end systolic volume, minus the forward stroke volume obtained from the aortic flow. ‘Backward power’ is the power loss due to backward flow and is the product of the backward volume, heart rate, mean right atrial pressure and the conversion factor 2.22*10^-6 (see Eq 1 in manuscript for explanation).

Loss of right ventricular power due to tricuspid regurgitation is shown in Table-Suppl 1. Note the large range, which is due to one patient (NYHA III) who had severe tricuspid regurgitation after destructive endocarditis on the tricuspid valve two years earlier. The loss of forward stroke volume was almost 50% in this patient! The power loss was 17%, resulting in a 20% loss of mechanical efficiency in this patient. However, the power loss in the other patients with tricuspid regurgitation was negligible and did not affect the RV mechanical efficiency significantly (P=0.22). Therefore, we can conclude that, except for the case with destructed tricuspid valves, moderate to severe tricuspid regurgitation had little to no consequences for the RV mechanical efficiency.
**RV $^{18}$FDG-PET and myocardial glucose uptake rate**

The $^{18}$FDG study occurred 1 day after the $^{15}$O-PET scans (Figure 1, main manuscript). Figure Suppl-1A displays the $^{18}$FDG scan preparation and PET protocol. The patients were prepared with overnight fasting, a single oral dose acipimox 250mg (Nycomed, Netherlands BV) and special carbohydrate and protein-enriched meal.3

*Data acquisition and image analysis* have been described previously.4 Briefly, The scan was performed in 3D acquisition mode using an ECAT EXACT HR+ scanner (Siemens/CTI, Knoxville, TN, USA). Two hours after administration of acipimox, a 10-min transmission scan was started to correct subsequent scan for tissue attenuation. Then, $^{18}$FDG (185 MBq) was injected intravenously and a dynamic emission scan started simultaneously (60 min, 39 frames). Venous blood was sampled to measure plasma glucose and free fatty acids during the scan. A similar re-slicing procedure of $^{15}$O-PET image processing as described in the main manuscript was undertaken for $^{18}$FDG images. RV wall ROIs were defined with the summed $^{18}$FDG short-axis image and used to generate time-activity curves by regions of interest projection onto the dynamic images.

*Myocardial glucose uptake rate* ($\text{MRglu}, \mu\text{mol glucose} / \text{gram cardiac tissue} / \text{min}$) was calculated using the Patlak method:5

$$= (K_i \ast \text{plasma glucose concentration}) / \text{lumped constant} \quad \text{(Suppl.-Eq. 1)}$$

where $K_i$ is the influx rate constant derived from the $^{18}$FDG time-activity-curve and was determined in the RV wall within the region of the blue line shown in Figure Suppl-1B. The lumped constant for cardiac $^{18}$FDG is considered 1 in our PET-center.
Despite the exclusion of patients with known diabetes mellitus, two patients (one NYHA II and one NYHA III) turned out to have hyperglycaemia (fasting glucose 16.8 ± 0.1 mmol/L), which persisted during the $^{18}$FDG scan. To avoid influence of hyperglycaemia on the calculation of MRglu, these two patients were excluded from further $^{18}$FDG-analysis. Mean plasma glucose at start $^{18}$FDG scan was 5.6 ± 0.8 (3.9-6.9, n=14) mmol/L, mean plasma free fatty acids was 0.65 ± 0.22 (range 0.33-1.04) mmol/L and was lowered after acipimox intake to 0.08 ± 0.03 (range 0.03-0.15, n=14) mmol/L as expected (normal value 0.3-0.9 mmol/L).

In Figure Suppl-1C the RV MRglu is plotted against the RV efficiency, showing no association between the two parameters. It must be taken into account that determination of RV MVO₂ (and power) occurred under near-fasting conditions, whereas patients underwent the $^{18}$FDG-scan under metabolic preparation to obtain maximal cardiac glucose uptake. Nevertheless, because the PET studies were standardized for all PAH patients, it can be concluded that the lack of correlation between RV efficiency and (maximal) glucose uptake is a true reflection for the whole group. In addition, should the metabolic shift have occurred to maximal glucose oxidation, mechanical efficiency would only increase with 8% maximally, as the caloric equivalent of glucose oxidation is 473 kJ/mol O₂ versus 439 kJ/mol O₂, by fatty acids oxidation. There was, however, no difference in glucose uptake rate between NYHA II and III patients, whereas RV efficiency reduced by 50% up to 4-fold in the severe PAH patient group compared to NYHA II.
RV power output of the normal right ventricle

The normal RV has a power output of about 0.16 J/s, assuming a mPAP of 12 mmHg and a cardiac output of 6 L/min. When compared to the normal heart, the hypertrophied RV power of both NYHA II and III patients is 4-fold higher (p=0.0001), as a result of an increased RV afterload in PAH (Figure Suppl-2). Assuming that RV efficiency remains stable at the beginning of the disease, MVO₂ should increase 4-fold, too, along with RV power. However, the RV power remains similar between the NYHA II and III patients, despite a lower cardiac output and stroke volume in NYHA III. The lower RV efficiency in NYHA III is due an increase of MVO₂, which almost doubled.
The interventricular septum plays an important role in RV power generation next to the RV free wall in PAH. To date, it is however not clear which part of the septum contributes to RV pumping and O₂ consumption in IPAH.

For this reason we show two alternative calculations of the RV mechanical efficiency, next to the results shown in the main manuscript. First, mechanical efficiency is calculated for the RV free wall alone, in which the MVO₂ of the total interventricular septum is not taken into account (Figure Suppl-3A). Secondly, Figure Suppl-3B shows the mechanical efficiency is calculated for the RV free wall including the MVO₂ of the total interventricular septum. In the latter, the overall mechanical efficiency is reduced by almost 50% compared to Fig. Suppl-3A. Despite different ways in calculating the RV efficiency, it had not effect on the proportional values between the two IPAH groups: the patients with severe IPAH (NYHA III) remained to have significantly reduced RV efficiency in comparison to the NYHA II patients.
**Supplement Table**

**Table Suppl-1**

<table>
<thead>
<tr>
<th>PAH pts (n = 6)</th>
<th>Median</th>
<th>Range</th>
</tr>
</thead>
<tbody>
<tr>
<td>Forward stroke volume (ml)</td>
<td>43.4</td>
<td>39.1 – 63.4</td>
</tr>
<tr>
<td>‘Backward’ volume (ml)</td>
<td>9.2</td>
<td>1.9 – 36.4</td>
</tr>
<tr>
<td>Percentage of total RV volume (%)</td>
<td>15.8</td>
<td>4.7 – 46.9</td>
</tr>
<tr>
<td>Forward RV power (J/s)</td>
<td>0.55</td>
<td>0.42 – 0.65</td>
</tr>
<tr>
<td>‘Backward’ RV power (J/s)</td>
<td>0.004</td>
<td>0.001 – 0.119</td>
</tr>
<tr>
<td>Percentage of total power (%)</td>
<td>0.72</td>
<td>0.38 – 17.6</td>
</tr>
</tbody>
</table>
Supplemental Figure Legends

Figure Suppl-1

Panel A Preparation protocol and time schedule of $^{18}$FDG-PET

Panel B Example of a summed $^{18}$FDG-image at basal plane in short-axis view of the same patient in Figure 2 (main manuscript). The MRglu in the RV wall of the shown patient (NYHA IV) in the figure was 0.31 $\mu$mol/g ventricular tissue /min. RV right ventricle, LV left ventricle.

Panel C Plot of RV myocardial glucose uptake rate (MRglu) against RV mechanical efficiency. There was no correlation between the two parameters ($r=-0.38$, $P=0.18$). Dotted line represents the best fit to the data.

Figure Suppl-2 Power output of NYHA II and III, as in Fig 3E. The line across the bar graph represents the power output of the normal right ventricle. *** $P=0.0001$ for both NYHA II and III.

Figure Suppl-3 Mechanical efficiency of IPAH patients with NYHA II and III calculated for only the RV free wall (Panel A) and RV wall plus total interventricular septum (Panel B).
Supplement Figures

**Figure Suppl-1A**

![Timeline Diagram](image)

**Figure Suppl-1B**

![Heatmap Image](image)

**Figure Suppl-1C**

![Scatter Plot](image)
Figure Suppl-2

![Graph showing comparison of Power (J/s) between normal RV for II and III with ns and *** annotations.](image-url)
Figure Suppl-3

A

p < 0.001

B

p = 0.004
Supplemental References


